

LECTURES ON THE MEDICAL ELECTRICAL EQUIPMENT SAFETY STANDARD: IEC 60601-1 BS EN 60601-1 (2006)

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USEFUL WEBSITES:

1. Articles on Electrical Safety under Articles section of Electronic and Biomedical Engineering website:
<http://www.ebme.co.uk>
2. Medical Devices section of the MHRA (Medicines and Healthcare products Regulatory Agency):
<http://www.mhra.gov.uk>
3. IEC (International Electrotechnical Commission)
<http://www.iec.ch/>
4. British Standards Online:
<https://bsol.bsigroup.com/en/BsolHomePage/>

HOW WE GOT TO WHERE WE ARE: A HISTORY OF (UK) ELECTRICAL SAFETY DOCUMENTS

**Hospital Technical Memorandum No. 8 (HTM8),
1963, Revised 1969.**

“Safety Code for Electromedical Apparatus.”
Department of Health and Social Security (DHSS),
London.

**Draft Standard of the International
Electrotechnical Commission (IEC), 1976.**

“General Requirements for Safety of Electrical
Equipment used in Medical Practice.”

Topic Group Report 24 (TGR24), 1977.

“A guide to Electrical Hazards and Safety
Standards.” The Hospital Physicists’ Association
(HPA).

Topic Group Report 25 (TGR25), 1977.

“A guide to Acceptance Testing of Electromedical
Equipment.” HPA.

**Health Equipment Information No. 95 (HEI95),
1981.** “Code of practice for acceptance testing of
medical electrical equipment.” DHSS

**Health Equipment Information No. 98 (HEI98),
1982.** “Management of equipment.” DHSS

BS 5724: Part 1: 1979.

(≡ IEC Publication 601-1)

Safety of Medical Electrical Equipment
(Superseded HTM8 in April 1981)

Topic Group Report 37 (TGR37), 1983.

“Safe Design and Construction of Electromedical Equipment.” HPA.

BS 5724: Part 1: 1989.

BS EN 60601-1:1990

(Issue 2, October 1997)

“Medical Electrical Equipment - Part 1. General requirements for safety.”

BS EN 60601-1:2006.

(Identical with IEC 60601-1:2005)

Medical electrical equipment –

Part 1: General requirements for basic safety and essential performance

ABOUT BS EN 60601-1:1990

Medical Electrical Equipment – Part 1. General requirements for safety.

- Existed as a guidance document for manufacturers of medical equipment (or, as some have said, solely for the test bodies).
- Not aimed at use in the hospital. Standard not useful or easily applicable in this context.
- Part 1 requirements may be over-ridden by those in Part 2.
- Part 2 consists of many documents covering specific equipment, where variations or additions are required.
- A “hurdle to get to know.
- Perhaps half a dozen basic principles.

BS EN 60601-1:2006

Medical electrical equipment - Part 1: General requirements for basic safety and essential performance.

For manufacturers, regulation bodies, independent certification bodies and professional users and beneficiaries of medical electrical equipment.

Revised and now in its third edition, BS EN 60601-1:2006 applies to medical electrical equipment intended to be used in the diagnosis, treatment, or monitoring of a patient or for compensation or alleviation of disease, injury or disability. This international standard focuses on the basic safety and essential performance of medical electrical equipment and medical electrical systems.

BS EN 60601-1:2006 encapsulates a large body of expertise on safety and performance from around the world, for the benefit of all:

- Manufacturers - who can satisfy many markets around the world with a single design
- Regulatory bodies and independent certification bodies who assess safety and performance
- The professional users, patients and disabled persons who depend on the equipment.

CHANGES INTRODUCED IN BS EN 60601-1:2006

- Name change because “essential performance” is related to safety (e.g. the accuracy of physiological monitoring equipment).
- Electrical requirements (and terminology) further aligned with those for IT equipment EN 60950-1.
- Requirement for a manufacturer to have a formal risk management process in place which complies with ISO standards.
- Not just protection against electrical hazards, but now must also consider:
 - Mechanical hazards
 - Unwanted and excessive radiation
 - Temperature and other hazards (fire, spillage, biocompatibility, interruption of power)
 - Accuracy of controls and equipment
 - Programmable electrical medical systems (PEMS)
 - Medical Electrical Systems

The standard = 200 pages + nearly 200 pages of explanatory annexes, e.g.
Annex A: General guidance and rationale.

WHY DO HOSPITAL STAFF NEED TO KNOW ABOUT BS EN 60601-1?

- To understand the nature of electrical hazards and the special cases relating to patients (Remember: “The Number One Rule of Medical Physics”).
- To undertake acceptance testing.
- To enable local construction or modification of equipment at the hospital (“modification technology”).
- To understand the implications of connecting equipment together into systems.
- To undertake routine electrical safety testing.

OUR AIMS:

- To conduct an in-depth study of the Standard.
- To become familiar with the terminology.
- To learn the philosophy behind the Standard.
- To learn about the test procedures possible and applicable in the hospital environment.

CE MARKING AND THE MEDICAL DEVICE DIRECTIVE

- Since 1 January 1996 all electrical devices sold in the EC must be CE marked to show compliance with current regulations.
- Medical Electrical Equipment is required to meet certain Electromagnetic Compatibility Requirements (EMC).
- Since June 1998, CE marking for Medical Electrical Equipment requires compliance with The Medical Devices Directive (MDD) “Council Directive 93/42/EEC” 1993.
- This has many requirements for Medical Electrical Equipment including compliance and type testing to 60601 series, and compliance of the manufacturer with Quality Management Practices.
- See lectures by Dr Steve Crook and Dr Julian Henty on: “Medical device regulations and the need for a Quality Management System”.

CE MARKING - IMPLICATIONS

- Illegal to buy non-CE marked equipment.
- Manufacturer needs to satisfy a “notified body”.
- = Main standards test houses e.g. BSI (British Standards Institute) for UK.
- Controlled by “authorised body” e.g. MHRA (Medicines & Healthcare products Regulatory Agency)

In the early years: Claims of widespread abuse of system:

- Blame another country’s test houses for inadequate testing.
- Some manufacturers simply included CE label without employing a test house to demonstrate compliance.
- Software changes.
- Instances of enforced suspension of production.

CE MARKING – PROBLEMS

1. Domestic equipment

No longer classed as medical equipment – so not required to comply.

Protective earth failure, damage to housings, hot surfaces, poor maintenance may compromise safety.

At present, medical need may still over-ride the desire or need to have all equipment comply with the standard.

2. Plain non-compliance

e.g. Vibrating pad wanted by Physiotherapy Department supplied by small US company – Not legally allowable now if not CE marked.

3. In-house designs and modifications

If a hospital builds or modifies equipment for it's own organisation, does it have to be CE marked? Not necessarily – but nevertheless, it must satisfy requirements of MDD.

4. Collaborative research projects

- Grey area.
- Ultimately required to satisfy an Ethics Committee.

TERMINOLOGY AND DEFINITIONS

60601-1:2006 Section 3 defines 139 terms

WHICH EQUIPMENT IS MEDICAL EQUIPMENT?

Electrical equipment having an APPLIED PART or transferring energy to or from the PATIENT or detecting such energy transfer to or from the PATIENT which is:

- a) provided with not more than one connection to a particular SUPPLY MAINS; and
- b) intend by its MANUFACTURER to be used:
 - 1) in the diagnosis, treatment, or monitoring of a PATIENT; or
 - 2) for compensation or alleviation of disease, injury or disability.

2006 Clause 3.63

DEFINED TERMINALS & CONDUCTORS (SCARY VERSION)

EN 60601-1 : 1990

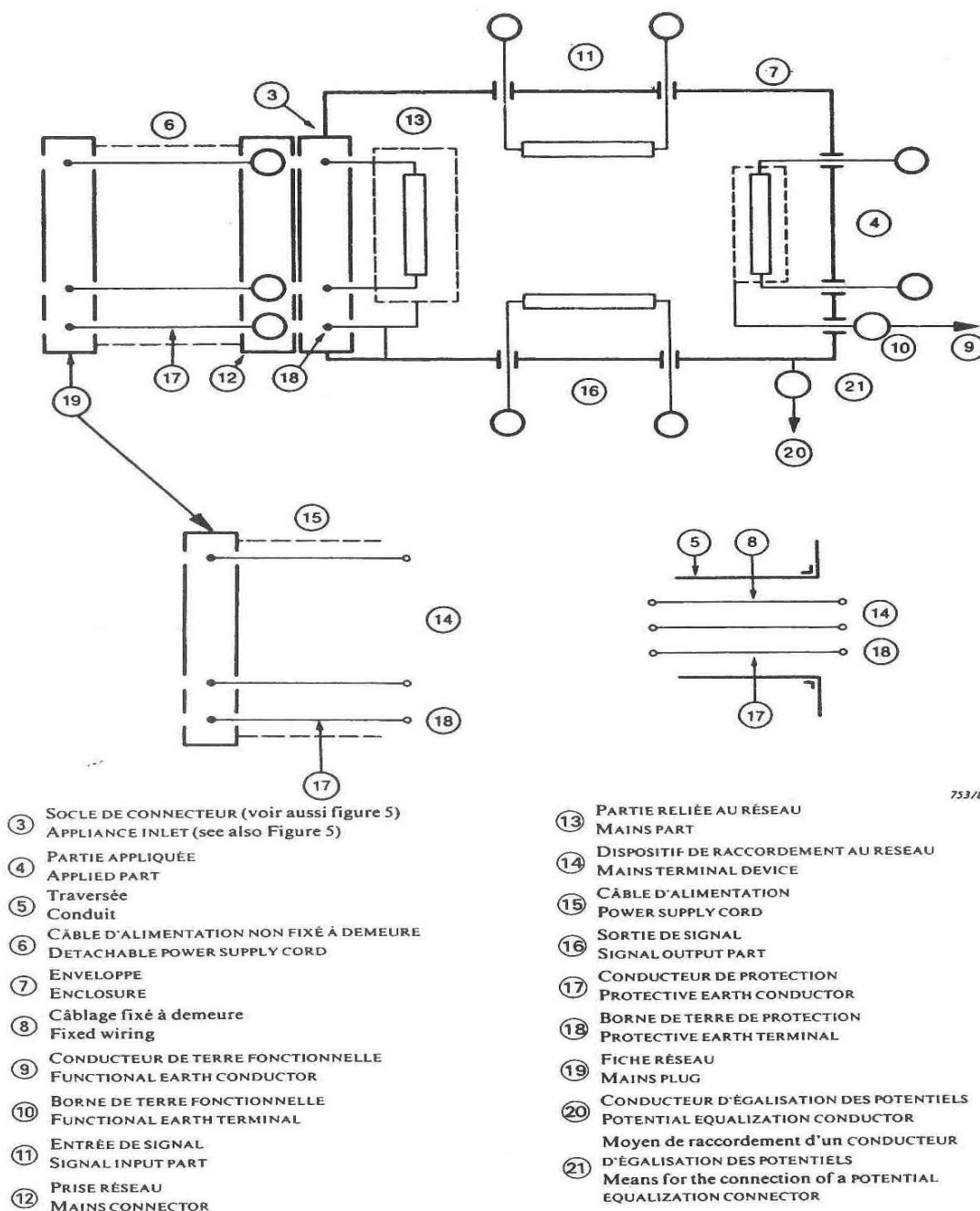
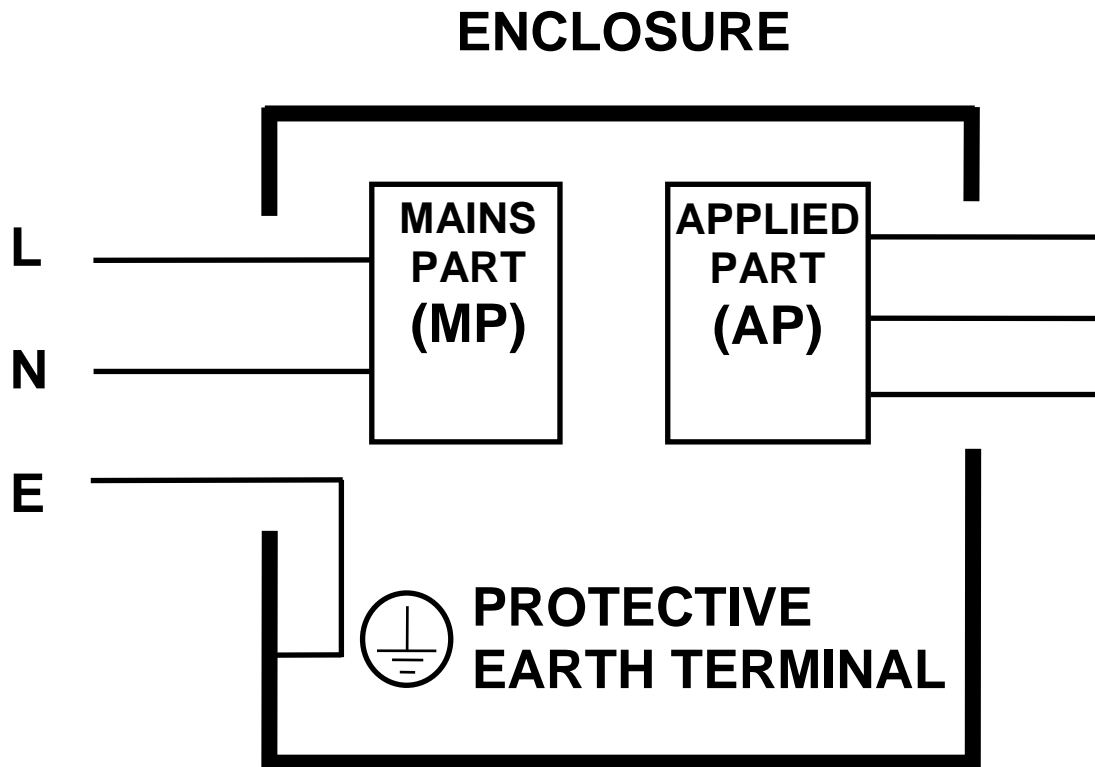


FIG. 1. — Exemple des conducteurs et des bornes définis (voir article 2).
Example of the defined terminals and conductors (see Clause 2).

Note: This becomes Figure 2 in
BS EN 60601-1:2006 (but without the French)

DEFINITIONS (FRIENDLY VERSION)



**INSTRUMENT UNDER TEST
(IUT)**

DEFINITIONS

ENCLOSURE:

Exterior surface of EQUIPMENT including:

- all ACCESSIBLE METAL PARTS, knobs and the like
- accessible shafts

1990 Clause 2.1.6

Exterior surface of electrical equipment or parts thereof

2006 Clause 3.26

NOTE: for the purpose of testing to this standard, metal foil, with specified dimensions, applied in contact with parts of the exterior surface made of material with low conductivity or made of insulating material is considered a part of the ENCLOSURE.

MAINS PART:

Electrical circuit that is intended to be connected to the SUPPLY MAINS.

NOTE 1: The MAINS PART includes all conductive parts that are not separated from the SUPPLY MAINS by at least one means of PROTECTION.

NOTE 2: For the purpose of this definition, the PROTECTIVE EARTH CONDUCTOR is not regarded as a part of the MAINS PART.

2006 Clause 3.49

APPLIED PART:

Part of the ME EQUIPMENT that in NORMAL USE: necessarily comes into physical contact with the PATIENT for ME EQUIPMENT or ME SYSTEM to perform its function.

+ NOTES 1, 2 and 3

2006 Clause 3.8

PATIENT CONNECTION:

Individual point on the APPLIED PART through which current can flow between the PATIENT and the ME EQUIPMENT in NORMAL CONDITION or SINGLE FAULT CONDITION.

2006 Clause 3.78

PROTECTIVE EARTH TERMINAL:

Terminal connected to conductive parts of CLASS I equipment for safety purposes. This terminal is intended to be connected to an external protective earthing system by a PROTECTIVE EARTH CONDUCTOR.

2006 Clause 3.95

METHOD OF PROTECTION AGAINST ELECTRIC SHOCK

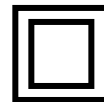
- **CLASS 1** equipment
Relies on protective earthing
Accessible metal parts cannot become live
- **CLASS 2** equipment
Relies on reinforced or double insulation
- Internally powered equipment is a separate Class

MNEUMONIC: CLASS I



Protective
Earthing

CLASS II



Double
Insulation

DEGREE OF PROTECTION AGAINST ELECTRIC SHOCK FOR THE APPLIED PART

3 TYPES – B, BF, CF

Differ in allowable leakage current

Different methods required for the F type



- **TYPE B APPLIED PART**

Any patient applied part may have a low impedance route to earth



- **TYPE BF APPLIED PART**

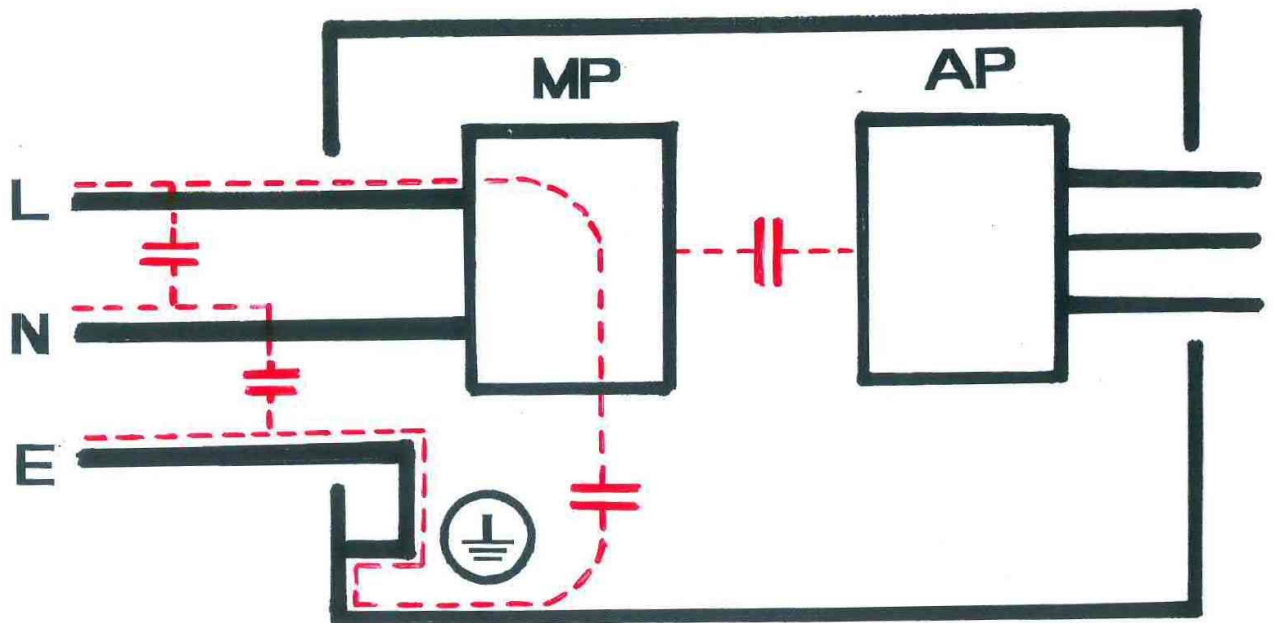
Has a floating (isolated or “earth-free”) patient applied part able to withstand a dielectric strength test (i.e. not just high impedance to earth)



- **TYPE CF APPLIED PART**

Similar to BF but with lower allowable leakage currents deemed to be safe even with connections directly to the heart

LEAKAGE CURRENT



DEMONSTRATIONS:

1. 100m mains extension lead
2. Transformer:
3. IEC mains inlet filters

LEAKAGE CURRENT:

Consider a capacitance between LIVE and the metal case connected to EARTH.

Reactance of a capacitor: $X_c = \frac{1}{\omega C} = \frac{1}{2\pi f C}$

$$\begin{aligned} |I| &= \frac{|V|}{X_c} = 2\pi f C V \\ &= 2\pi \times 50 \times 240 \times C \\ &= 7.5 \times 10^4 C \end{aligned}$$

	C	X_c at 50Hz	I
Transformer: Primary to chassis	100pf	32M Ω	7.4 μ A
“Medical grade” IEC filter capacitors	3300pF	960k Ω	240 μ A
100m mains cable: L to E	11nF	290k Ω	0.8mA
IEC filter capacitors	47nF (0.047 μ F)	67k Ω	3.4mA
Dangerous “homemade” filter	1.5 μ F	2.1k Ω	110mA

DEGREE OF PROTECTION AGAINST ELECTRIC SHOCK FOR THE APPLIED PART

3 TYPES – B, BF, CF

Differ in allowable leakage current

Different methods required for the F type



- **TYPE B APPLIED PART**

Any patient applied part may have a low impedance route to earth



- **TYPE BF APPLIED PART**

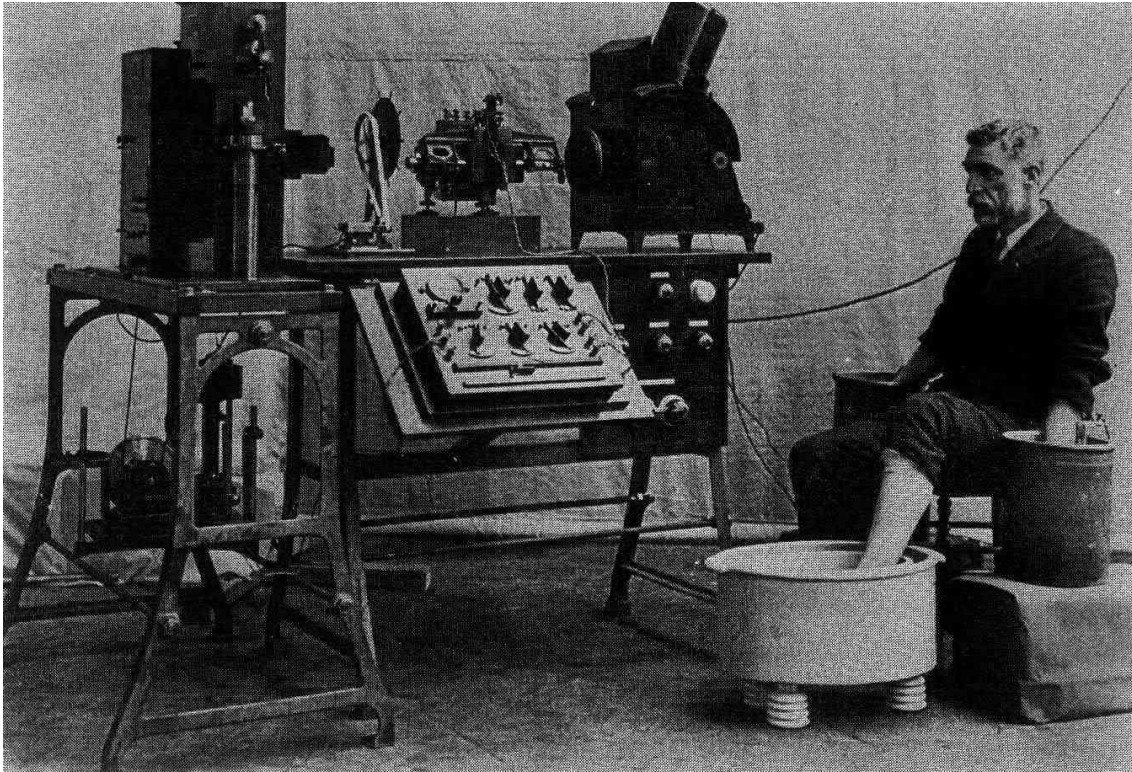
Has a floating (isolated or “earth-free”) patient applied part able to withstand a dielectric strength test (i.e. not just high impedance to earth)



- **TYPE CF APPLIED PART**

Similar to BF but with lower allowable leakage currents deemed to be safe even with connections directly to the heart

THE FIRST (COMMERCIAL) ELECTROCARDIOGRAPH 1912



EVOLUTION OF THE ECG AMPLIFIER CIRCUIT

1946

1962

1967

Figures 8, 9, and 10 show evolution of Electrocardiograph Amplifier Circuit.

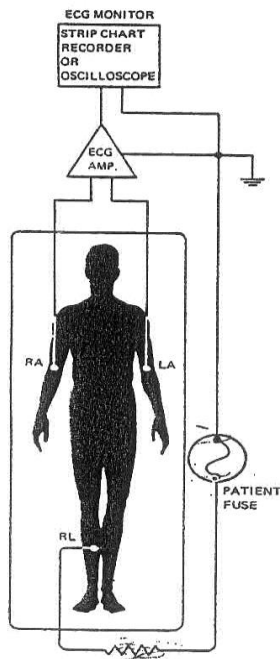


FIGURE 8. Ground Referenced Differential Electrocardiograph Amplifier

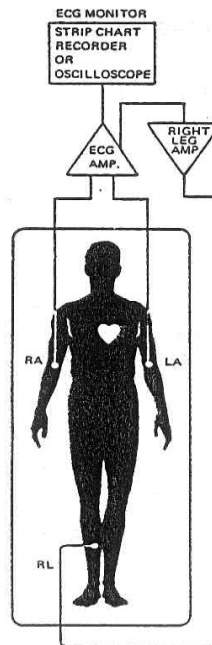


FIGURE 9. Driven Right Leg Electrocardiograph Amplifier

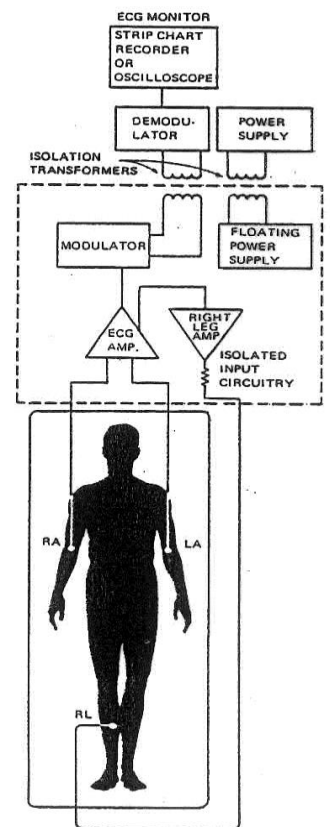
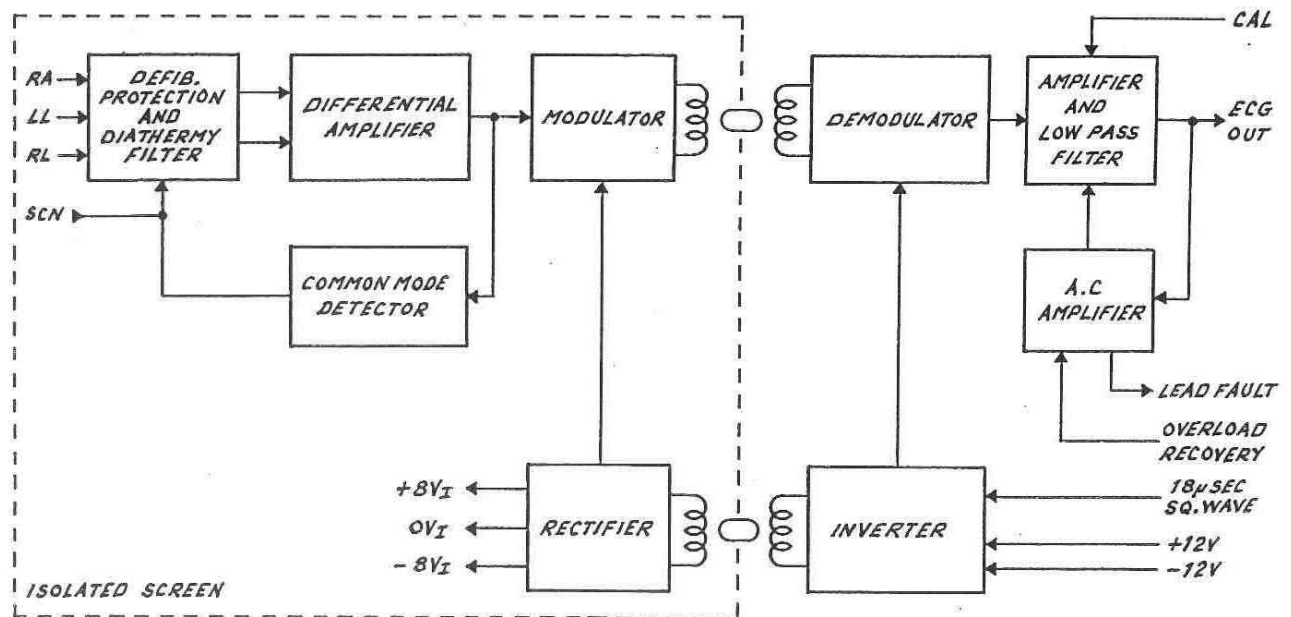


FIGURE 10. Isolated Input Electrocardiograph Amplifier













KONE CARDIAC MONITOR 573 ECG AMPLIFIER BLOCK DIAGRAM



More detail in the UCL MSc in Physics and
Engineering in Medicine (PEM) module:
MPHYGB20 Medical Electronics and Control

MARKINGS ON MEDICAL ELECTRICAL EQUIPMENT

APPENDIX B

 <p>1. ATTENTION! CONSULT ACCOMPANYING DOCUMENTS</p>	 <p>2a. PROTECTIVE EARTH</p>	 <p>2b. FUNCTIONAL EARTH</p>
<p><u>PROTECTION CLASS I & CLASS II EQUIPMENT</u></p>		
<p>NOTE THERE IS NO SYMBOL FOR CLASS I EQUIPMENT</p>	 <p>3. CLASS II EQUIPMENT</p>	
 <p>4. ANAESTHETIC-PROOF EQUIPMENT</p>	 <p>5. ANAESTHETIC-PROOF CATEGORY G</p>	
 <p>6. TYPE B EQUIPMENT</p>	 <p>7. TYPE B WITH DEFIBRILLATOR PROTECTION</p>	
 <p>8. TYPE BF EQUIPMENT</p>	 <p>9. TYPE BF WITH DEFIBRILLATOR PROTECTION</p>	
 <p>10. TYPE CF EQUIPMENT</p>	 <p>11. TYPE CF WITH DEFIBRILLATOR PROTECTION</p>	

“OHMWORK”

WHAT "TYPE" CLASSIFICATIONS WOULD BE APPROPRIATE FOR THE FOLLOWING EQUIPMENT:

1. A cardiac monitor recording ECG from surface electrodes attached to a critically ill patient fitted with a central venous pressure catheter.
2. A pulse oximeter.
3. A pressure measuring system in a cardiac catheterisation laboratory.
4. A peristaltic infusion pump.
5. An electronic thermometer for measuring skin temperature.
6. An infra-red therapy lamp.

SINGLE FAULT CONDITIONS:

A condition in which a single means for reducing a RISK is defective or a single external abnormal condition is present.

2006 Clause 3.116 (See also 4.7 and 13.2)

The following are defined as SINGLE FAULT CONDITIONS:

- Interruption of a PROTECTIVE EARTH CONDUCTOR
- Interruption of one supply conductor
- Appearance of an external voltage on an F-TYPE APPLIED PART
- Appearance of an external voltage on a SIGNAL INPUT or SIGNAL OUTPUT

NOTE:

Earthing of a PATIENT is considered a NORMAL CONDITION.

Reversal of the MAINS SUPPLY is not considered as a fault, but must be tested for.

LEAKAGE CURRENT DEFINITIONS:

“Current that is not functional.”

2006 Clause 3.47

1. EARTH LEAKAGE CURRENT

Flows from the MAINS PART through or across the insulation into the PROTECTIVE EARTH CONDUCTOR.

2006 Clause 3.25

- Equipment powered from mains via tester MD in line with earth connection
- Only appropriate for Class I equipment

2. TOUCH CURRENT (FORMERLY KNOWN AS “ENCLOSURE LEAKAGE CURRENT”)

Flows from the ENCLOSURE ... through an external CONDUCTIVE CONNECTION other than the PROTECTIVE EARTH CONDUCTOR to earth or another part of the ENCLOSURE.

2006 Clause 3.129

- Equipment powered from mains via tester MD between points on enclosure and tester earth (not the equipment protective earth)
- Class I and II

3. PATIENT LEAKAGE CURRENT

Flows from the PATIENT CONNECTIONS via the PATIENT to earth.

2006 Clause 3.63

4. PATIENT LEAKAGE CURRENT (MAINS ON APPLIED PART)

Originating from the unintended appearance of a voltage from an external source on the PATIENT and flowing from the PATIENT via the PATIENT CONNECTIONS of an F-TYPE APPLIED PART to earth

2006 Clause 3.63

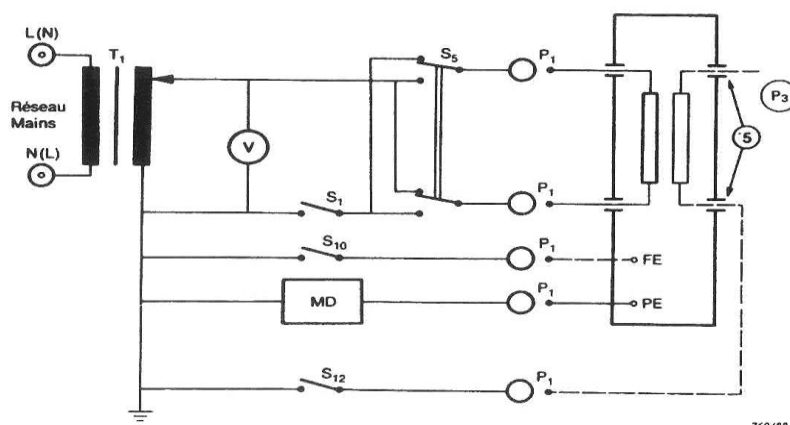
5. PATIENT AUXILIARY CURRENT

Flows in the PATIENT in NORMAL USE between any PATIENT CONNECTION and all other PATIENT CONNECTIONS and not intended to produce a physiological effect.

2006 Clause 3.77

MEASURING EARTH LEAKAGE CURRENT (SCARY VERSION)

EN 60601-1 : 1990



Voir légendes page 243

See legends page 243

Mesure dans toutes les combinaisons possibles des positions de S_5 , S_{10} et de S_{12} avec:

S_1 fermé (CONDITION NORMALE), et
 S_1 ouvert (CONDITION DE PREMIER DÉFAUT)
 et pour les mesurages selon le paragraphe 19.4a), tableau IV, notes 1 à 4 inclus
 S_1 ouvert (CONDITION DE PREMIER DÉFAUT)

Measure in all possible combinations of positions of S_5 , S_{10} and S_{12} with:

S_1 closed (NORMAL CONDITION), and
 S_1 open (SINGLE FAULT CONDITION)
 and for measurement in accordance with Sub-clause 19.4a), Table IV, notes 1 up to and including 4
 S_1 open (SINGLE FAULT CONDITION)

FIG. 16. — Circuit de mesure pour le COURANT DE FUITE À LA TERRE d'un APPAREIL DE LA CLASSE I, avec ou sans PARTIE APPLIQUÉE (voir paragraphe 19.4f) et notes du tableau IV).

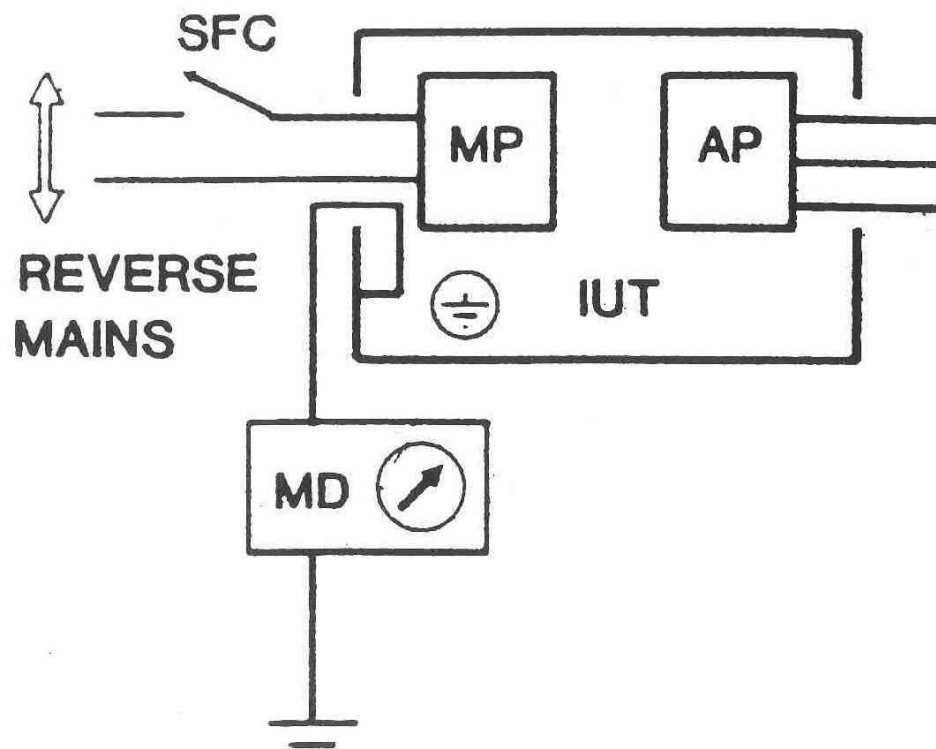
Exemple avec le circuit d'alimentation de mesure de la figure 10.

Measuring circuit for the EARTH LEAKAGE CURRENT of CLASS I EQUIPMENT, with or without APPLIED PART (see Sub-clause 19.4f) and notes to Table IV).

Example with the measuring supply circuit of Figure 10.

Note: This becomes Figure 13 in
BS EN 60601-1:2006

1. EARTH LEAKAGE CURRENT



Class 1
Type B,BF,CF

Flows from the MAINS PART through or across the insulation into the PROTECTIVE EARTH CONDUCTOR.

2006 Clause 3.25

- Equipment powered from mains via tester MD in line with earth connection
- Only appropriate for Class I equipment

THE MEASURING DEVICE (MD)

EN 60601-1 : 1990

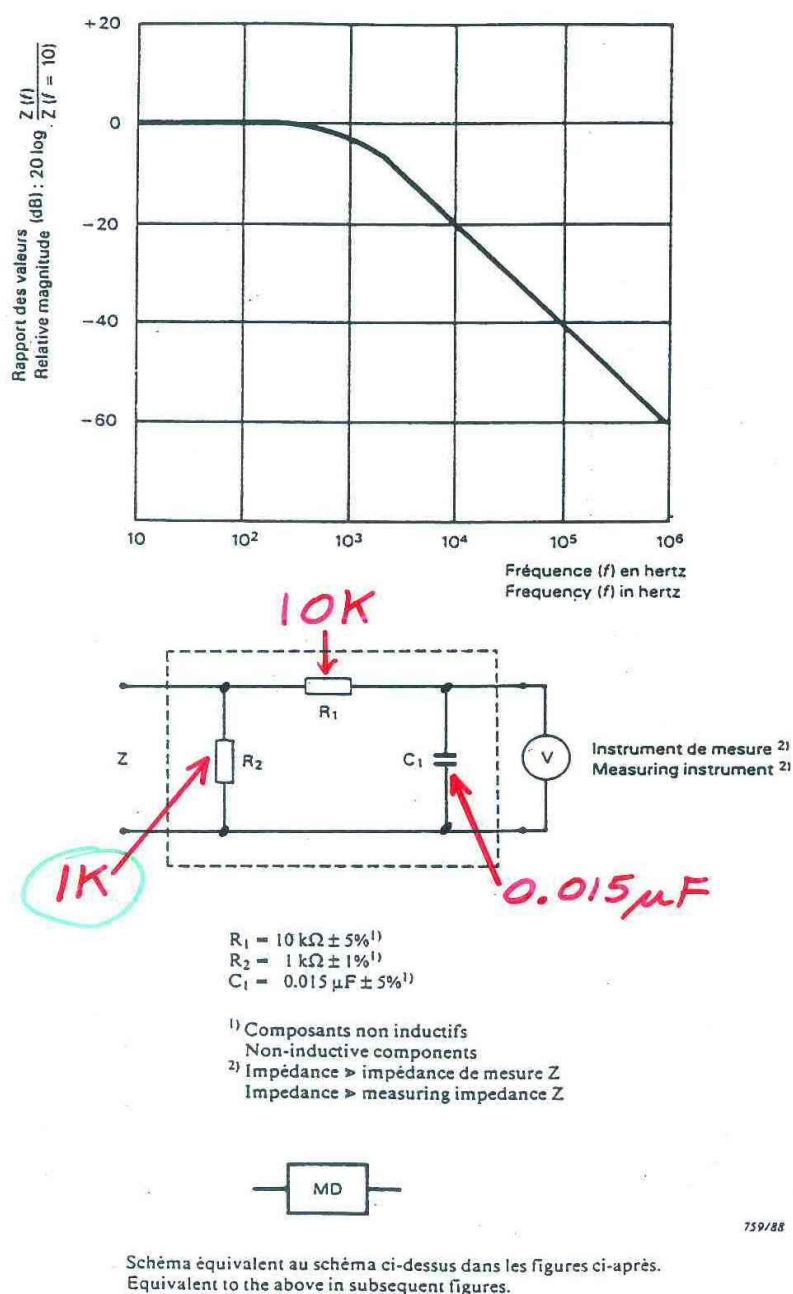
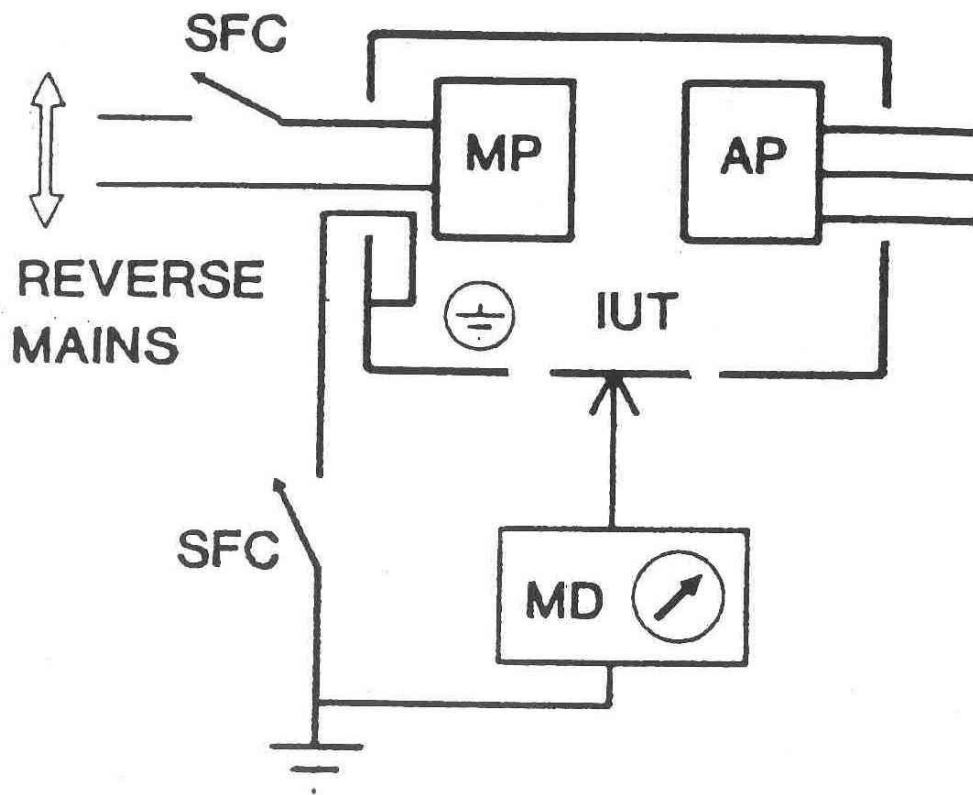


FIG. 15. — Exemple d'un dispositif de mesure et de sa caractéristique de fréquence (voir paragraphe 19.4e)).
Example of a measuring device and its frequency characteristic (see Sub-clause 19.4e)).

Note: This becomes Figure 12 in 60601-1:2006

2. TOUCH CURRENT (FORMERLY KNOWN AS “ENCLOSURE LEAKAGE CURRENT”)



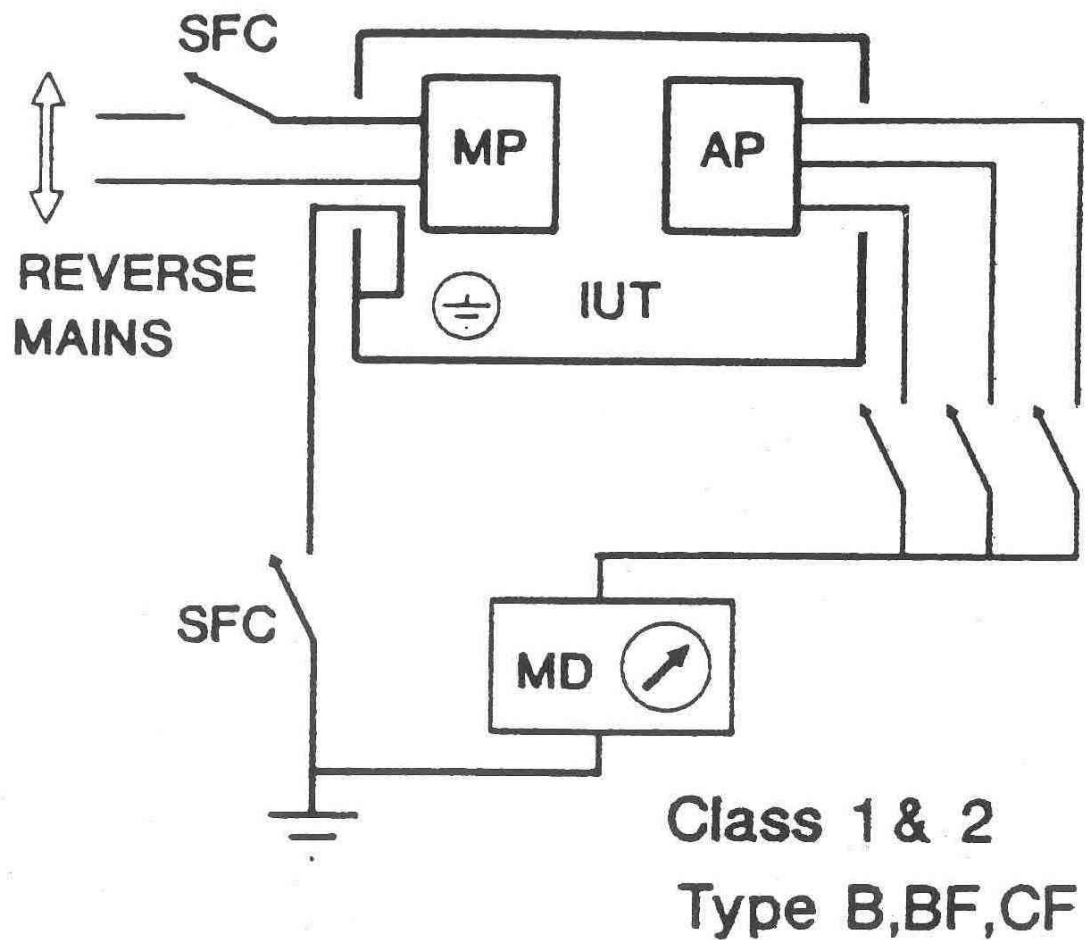
Class 1 & 2
Type B,BF,CF

Flows from the ENCLOSURE ... through an external CONDUCTIVE CONNECTION other than the PROTECTIVE EARTH CONDUCTOR to earth or another part of the ENCLOSURE.

2006 Clause 3.129

- Equipment powered from mains via tester MD between points on enclosure and tester earth (not the equipment protective earth)
- Class I and II

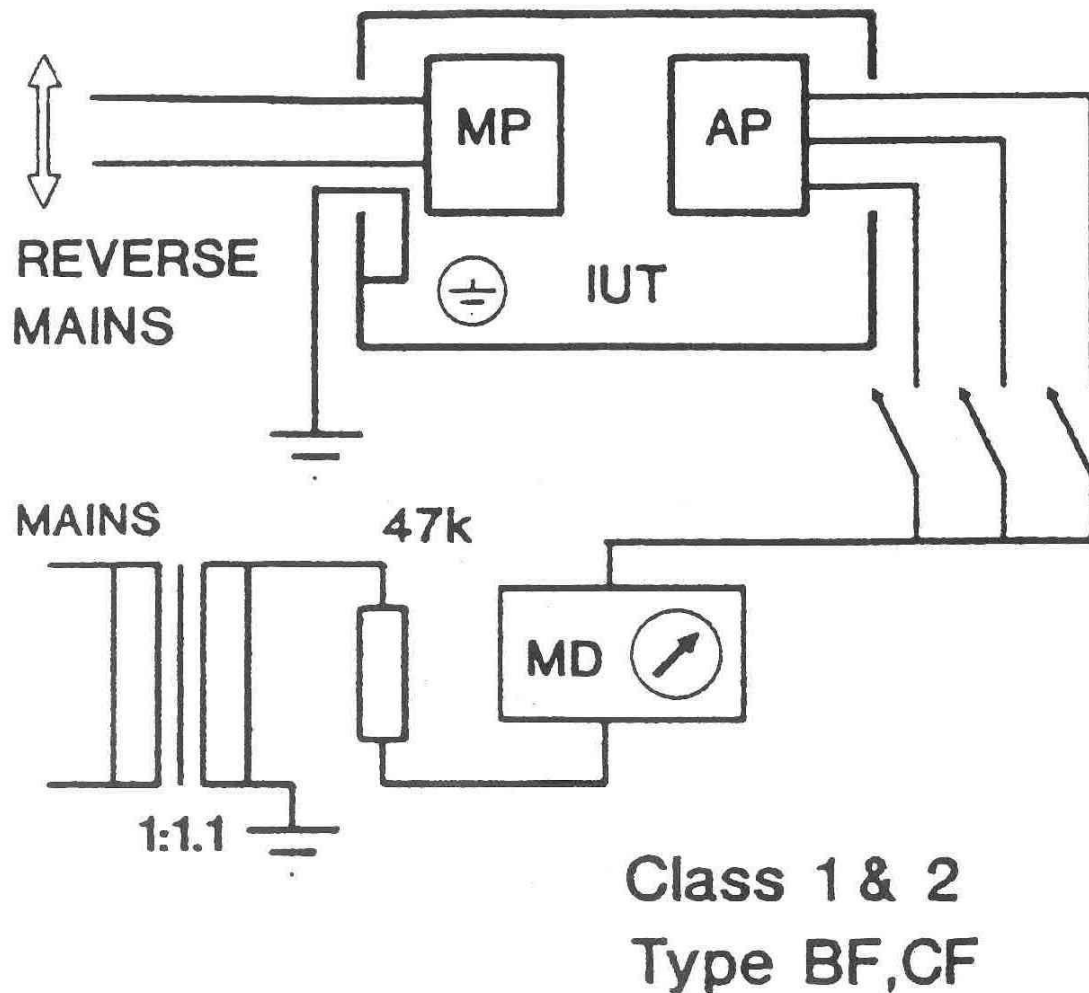
3. PATIENT LEAKAGE CURRENT



Flows from the PATIENT CONNECTIONS via the PATIENT to earth.

2006 Clause 3.63

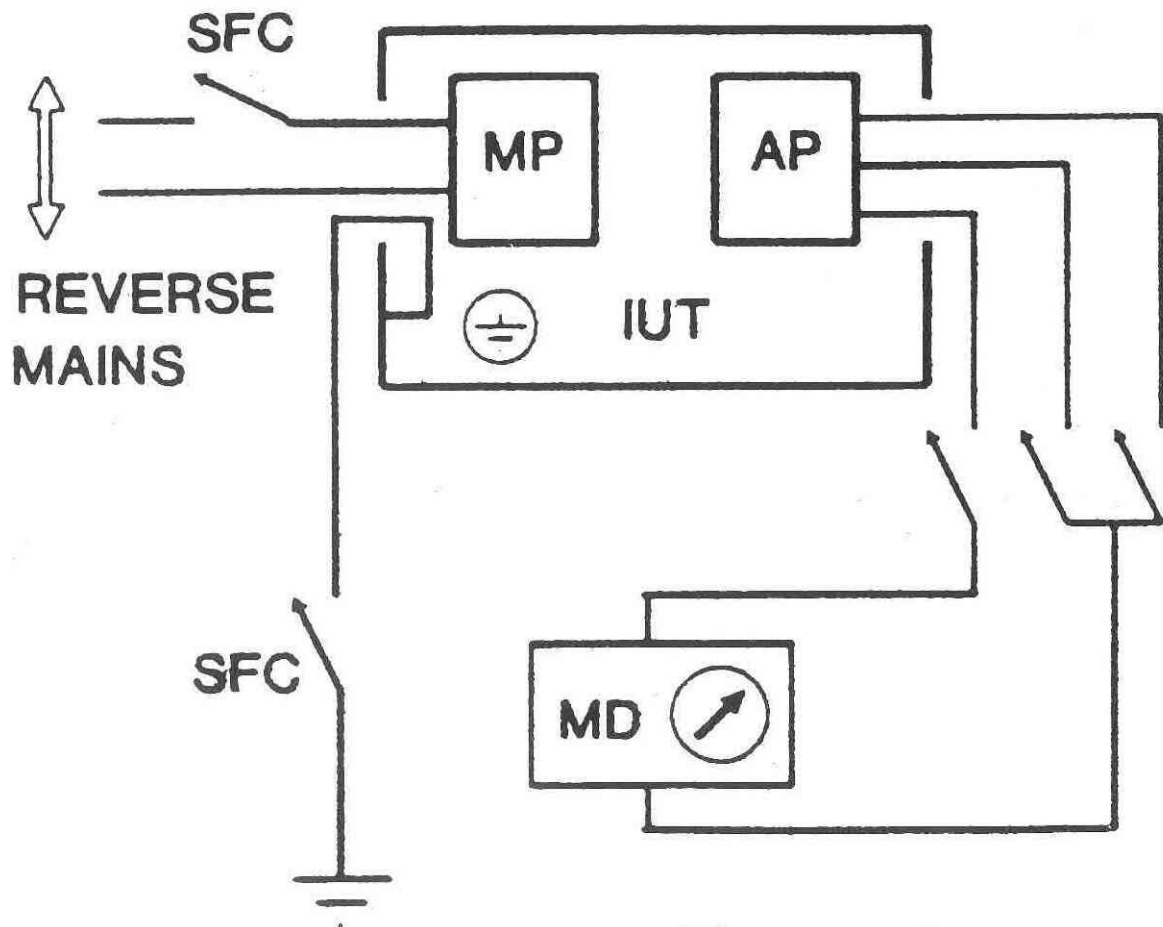
4. PATIENT LEAKAGE CURRENT (MAINS ON APPLIED PART)



Originating from the unintended appearance of a voltage from an external source on the PATIENT and flowing from the PATIENT via the PATIENT CONNECTIONS of an F-TYPE APPLIED PART to earth

2006 Clause 3.63

5. PATIENT AUXILIARY CURRENT



Class 1 & 2
Type B,BF,CF

Flows in the PATIENT in NORMAL USE between any PATIENT CONNECTION and all other PATIENT CONNECTIONS and not intended to produce a physiological effect.

2006 Clause 3.77

Example 1: Obtain breathing rate by passing a small current through ECG electrodes and measuring ΔZ .

Example 2: Surgical diathermy plate “fall-off” detector.

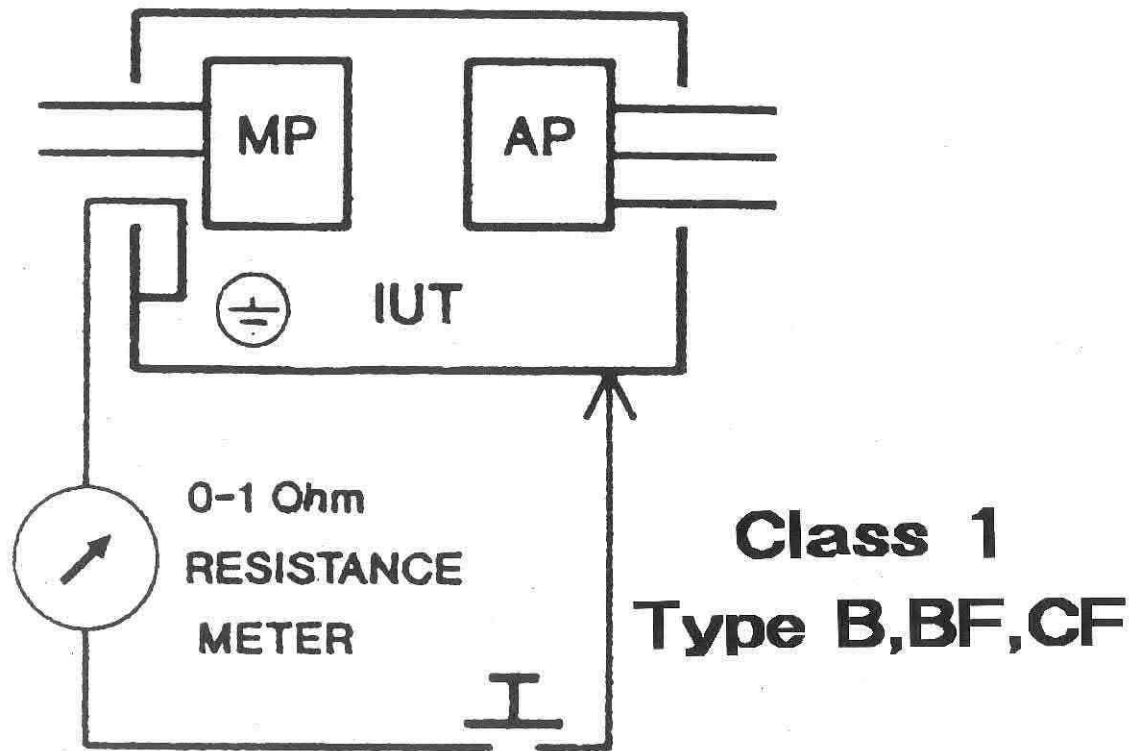
MAXIMUM ALLOWABLE LEAKAGE CURRENTS (mA) BS EN 60601-1: 2006

		Type B Applied Part		Type BF Applied Part		Type CF Applied Part	
		NC	SFC	NC	SFC	NC	SFC
Earth Leakage Current		0.5 5	4 10	0.5 5	4 10	0.5 5	4 10
Touch Current		0.1	0.5	0.1	0.5	0.1	0.5
Patient Leakage Current	DC AC	0.01 0.1	0.05 0.5	0.01 0.1	0.05 0.5	0.01 0.01	0.05 0.05
Patient Leakage Current (mains on applied part)					5		0.05
Patient Auxiliary Current	DC AC	0.01 0.1	0.05 0.5	0.01 0.1	0.05 0.5	0.01 0.01	0.05 0.05

NOTES ON TABLE OF MAXIMUM ALLOWABLE LEAKAGE CURRENTS

1. Earth Leakage Current and Touch Current relate to the enclosure – and not dependent on Type of Applied Part.
2. Maximum allowable ELC for NC and SFC increased by factor of 10 compared with BS EN 60601-1:1990.
3. Patient Leakage Current and Patient Auxiliary Current maximum limits are lower for DC compared with AC because of electrolysis.
4. Patient Leakage Current and Patient Auxiliary Current AC maximum limits for Type CF Applied Parts are lower compared with Type B and BF Applied Parts.
5. “No entries” for Patient Leakage Current (mains on applied part) because it is not an appropriate test for Type B Applied Parts AND it is not a NC – it is a SFC.

EARTH CONTINUITY



- **For equipment with an appliance inlet:**

Resistance between:

Conductive parts of the equipment and the protective earth terminal $\leq 0.1 \text{ Ohm}$

- **For equipment with a non-detachable power supply cord:**

Resistance between:

Conductive parts of the equipment and the earth pin of the mains plug $\leq 0.2 \text{ Ohm}$

EARTH CONTINUITY

BS EN 60601-1:1990 states:

“Compliance is checked by the following test:

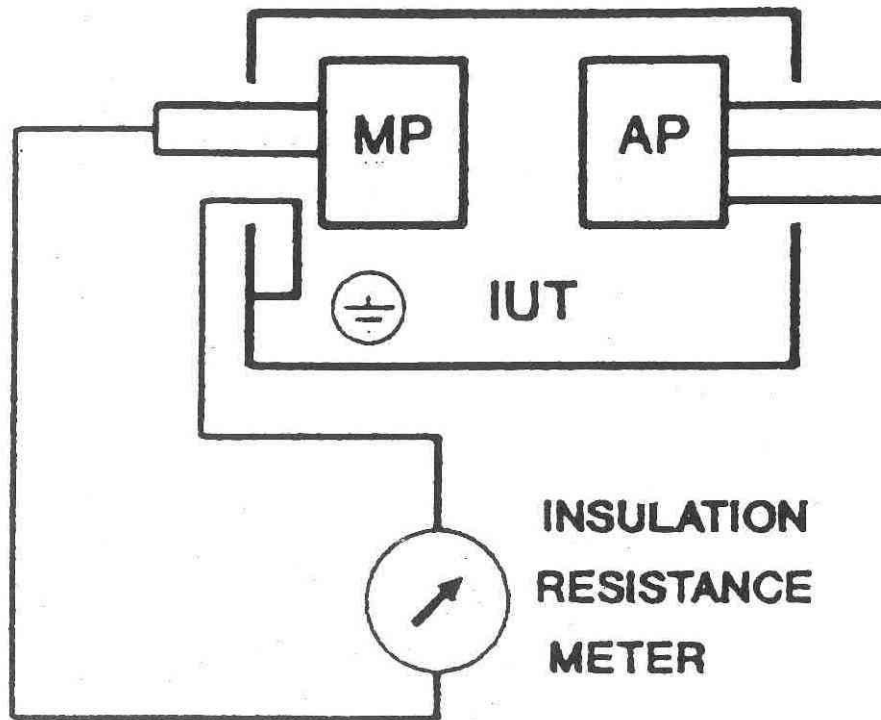
A current of 25 A or 1,5 times the rated current of the EQUIPMENT, whichever is greater ($\pm 10\%$), from current source with a frequency of 50 Hz or 60 Hz with a no-load voltage not exceeding 6 V is passed for 5 s to 10 s through the PROTECTIVE EARTH TERMINAL or the protective earth contact in the APPLIANCE INLET or the protective earth pin in the MAINS PLUG and each ACCESSIBLE METAL PART which could become LIVE in case of failure in BASIC INSULATION.

The voltage drop between the parts described is measured and the impedance determined from the current and voltage drop. It shall not exceed the values indicated in this sub-1990 Clause.”

1990 Clause 18f

“Ohmwork”: How does this compare with the 2006 version of the standard?

INSULATION RESISTANCE MAINS PART



Class 1

Type B,BF,CF

- Use 500V DC insulation tester (BS EN 60601-1 specifies “Dielectric Strength Test” – potentially destructive)
- Measure between earth pin and L & N connected together
- Any equipment switch in ON position
- Not less than 50 Megohms
- If substantially lower, investigate with manufacturer

QUESTION:
WHY DO WE NEED 500V
TO MEASURE RESISTANCES
> 50 MΩ?

Ohm's Law:

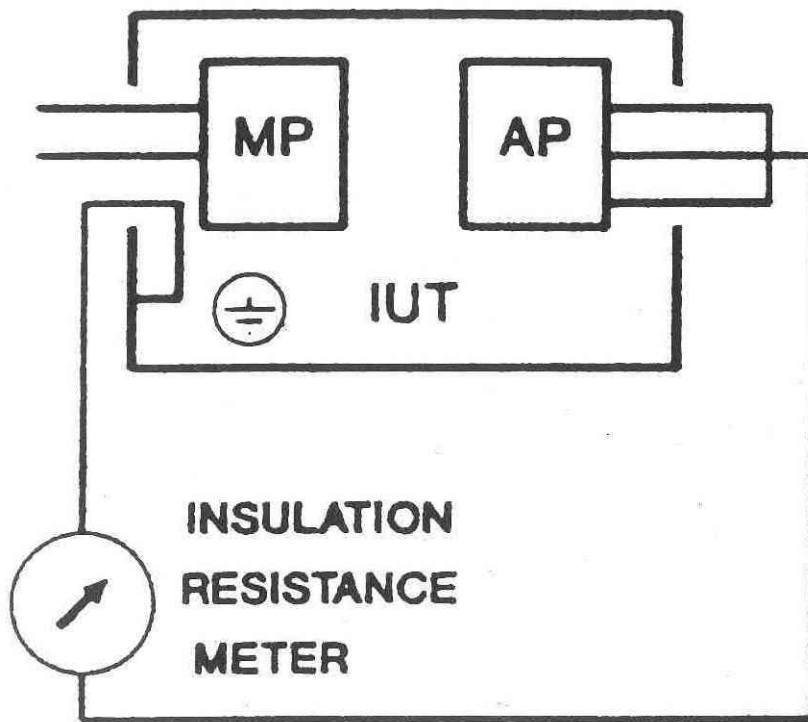
$$V = I \cdot R$$

$$I = \frac{V}{R}$$

$R = 50\text{M}\Omega$		
$V = 9\text{V}$	$V = 500\text{V}$	$V = 1000\text{V}$
$I = 0.18\mu\text{A}$	$I = 10\mu\text{A}$	$I = 20\mu\text{A}$

ANSWER:
SO THAT AN EASILY
MEASURABLE CURRENT
FLOWS

INSULATION RESISTANCE APPLIED PART



Class 1
Type BF,CF

- Use 500V DC insulation tester
- Measure between applied parts and earth connection
- Not less than 50 Megohms

PERSPECTIVE

Each hospital typically spends around £100,000 per year on electrical safety testing.

Number of deaths per year in UK due to:

- ELECTRICITY ? ~ 200
Many know electricity is a hazard
But don't understand the nature of the hazard
Most deaths relate to water & restricted movement
- MURDER ? ~ 200
- ROAD ACCIDENTS ? ~ 2000
- MEDICAL ELECTRICAL EQUIPMENT ?

THE MICROSHOCK SCARE

- 1960's equivalent of Y2K, BSE and GM food
- Concern that some catheterized patients were electrocuted by small, imperceptible currents
- Peak: Carl Walter (1970) and Ralph Nader (1971) claimed 1200 Americans electrocuted each year during diagnostic & therapeutic procedures

Comprehensive review of 25 years by 2 Canadian anaesthetists (Bruner and Leonard 1989) found only 4 deaths that could be attributed to these small currents:

- 3 prior to 1961
- Most recent in 1970.

John M. R. Bruner and Paul F. Leonard
Electricity, Safety and the Patient
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Some unnecessary precautions, but many improvements:

- Electrically isolated patient connections
- Manufacturers "groomed" to meet standards
- Education on safety for medical personnel
- Medical equipment testing procedures

INTRINSIC SAFETY

So that the possibility of being injured can't arise.

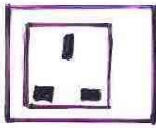
- 2mm plug patient lead problem

Between 1985 and 1994 24 children received severe electric shocks from patient leads being plugged into IEC connectors that “looked like” ECG head-boxes.

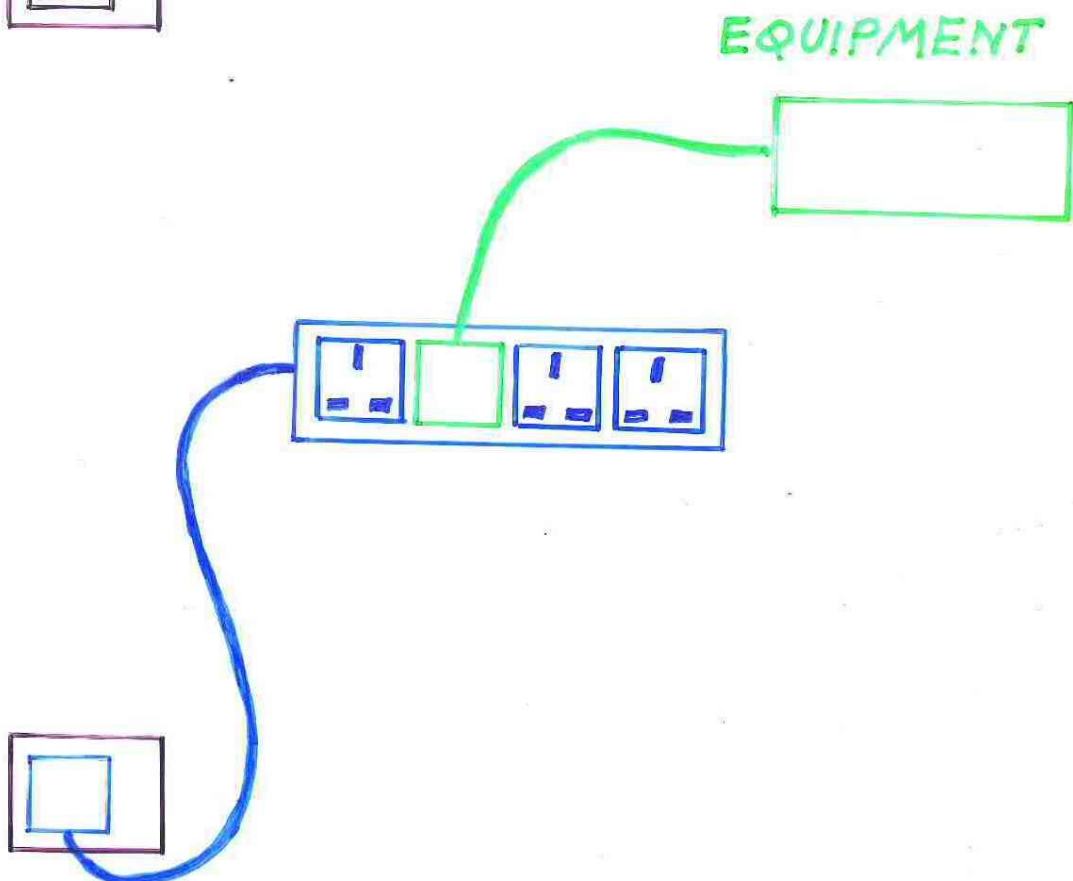
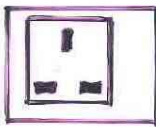
- Electric lawn mower connectors
- 3-pin IEC connector wired with 2-core mains cable
- Mains plug connected on each end of a cable

E.g. Extension lead made by film crew

The greatest risk
is related to the mains lead.

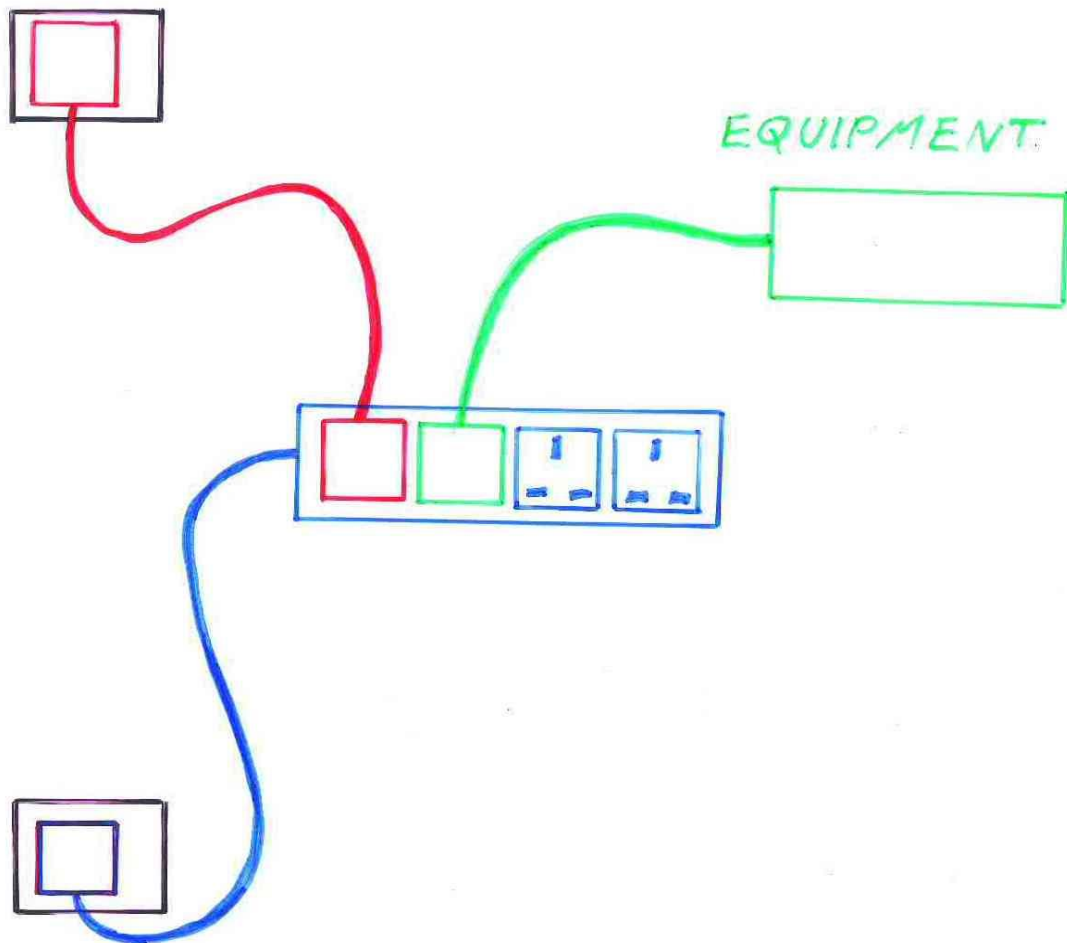


FILM CREW'S EXTENSION LEAD





FILM CREW'S EXTENSION LEAD



Blocked oxygen tubes 'faulty'

THE cause of five cases involving blocked oxygen tubes in hospitals has revealed they were more likely to be caused by faulty equipment than sabotage, police said yesterday. But the investigation has yet to 'necessarily provide a satisfactory explanation' to all the incidents. Tony Clowes, nine, from Dagenham, died after an oxygen pipe at Broomfield Hospital, Chelmsford became blocked.

INSPECTION

Majority of equipment faults

- mains lead
- found by visual inspection

Some automatic safety testers perform 40 or more tests

- a complete waste of time ??

No, but:

“A quick inspection and shake is worth as much as or more than 40 automated tests.”