MPHY3892 Radiobiology

Lecture 2

Cellular Effects, Target Theories and Survival Curves

Cell Death

INTERPHASE DEATH (after a dose of several hundred Gy)

- Cessation of metabolic activity
- Disintegration

REPRODUCTIVE DEATH

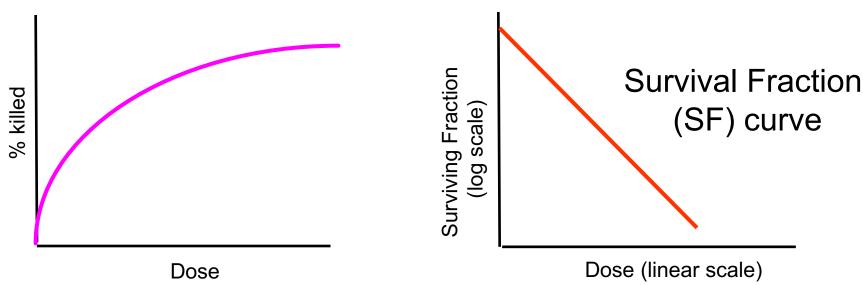
(after a dose of a few Gy)

- Inhibition of ability to divide
- Loss of ability to proliferate
- Occurs at the next or subsequent mitosis

Reproductive Death

- In radiobiology there is an emphasis on reproductive death
- Concept of reproductive death is not applicable to differentiated cells that no longer divide and are very resistant to radiation
- In radiotherapy: a tumour is locally controlled when ALL its cells have lost their power for indefinite proliferation
- In radiation protection of acute effects of radiation: regeneration of a damaged normal tissue depends on the number of survived stem cells

Survival Curves for Viruses and Bacteria



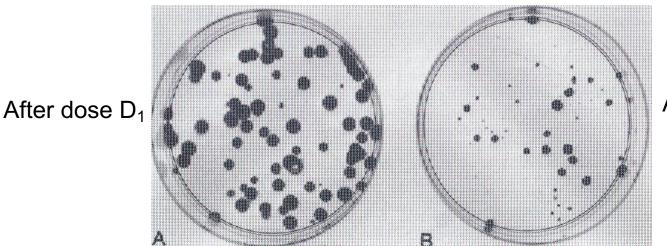
Surviving Fraction versus Dose is plotted in semi-logarithmic co-ordinates

Killing is random \Rightarrow statistical law of Poisson:

the proportion of surviving cells is e^{-p} , where p is a mean number of lethal events per cell

Generating *in-vitro* Surviving Fraction Curves

- A suspension of single cells in culture is grown at 37°C in Petri dishes in aseptic conditions
- Cells attach to surface
- Cells are irradiated to different doses
- Surviving cells divide and establish cell lines
- After several weeks most cells become exhausted and die
- Some cell lines are able to multiply quasi-indefinitely



After dose $D_2 > D_1$

Target Theories

- Are developed to link physical facts about radiation absorption with the observed surviving fraction curves
- Propose radiation sensitive <u>targets</u> within cells which have to be <u>hit</u> for the cell to die

Single Hit, Single Target Model

- Assumes a single hit to a single target is enough to kill a cell
- Results in an exponential Survival Fraction curve

$$N = N_0 e^{-D/D_0}$$

Exponential survival curves:

- for viruses, bacteria
- for certain types of mammalian cells

$$N = N_0 e^{-D/D_0}$$

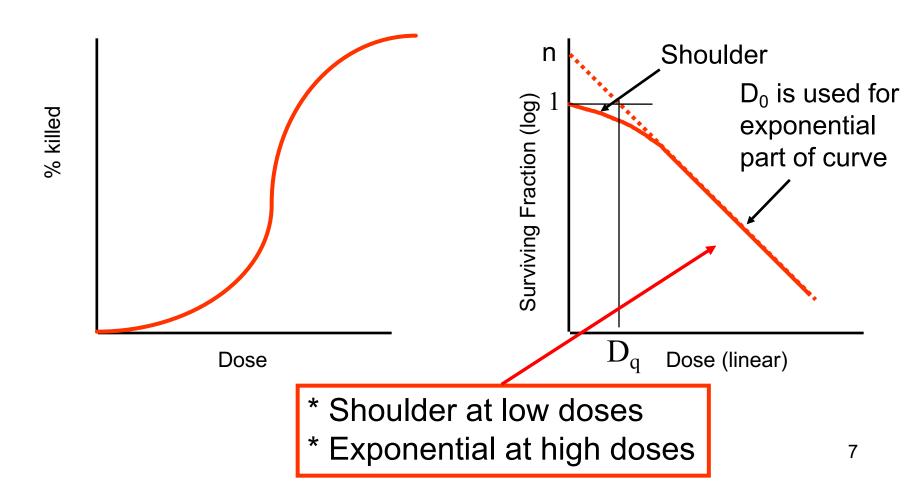
 N_0 is the initial number of cells

- **D**₀ mean lethal dose
 - gives the slope of the line
 - is the dose required to reduce the SF to 37%
 - is the dose required, on average, to put one hit in each cell
 - varies with cell type and type of radiation

For X-rays and γ -rays:

D₀ = 1500 Gy for viruses100 Gy for bacteria1 Gy for mammalian bone marrow stem cells

Mammalian Cell SF Curve



Mammalian Cell SF Curve

D₀ only refers to exponential part

$$D_0 = 1 - 2 Gy$$

Extrapolation number n

$$n = 1 - 5$$

• Quasi threshold dose D_q where extrapolation crosses SF=1 line \Rightarrow is the measure of the size of shoulder

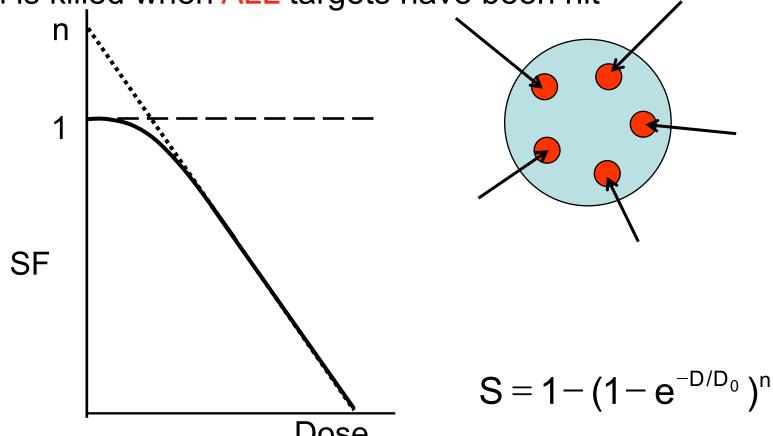
$$D_{q} = 0.5 - 2.5 \text{ Gy}$$

Not a simple single hit, single target model

Single Hit, Multi-Target Model

- Cell contains n identical targets
- Each target is inactivated by ionisation
- Individual target inactivation is not lethal

Cell is killed when ALL targets have been hit



Single Hit, Multi-Target Model

$$S = 1 - (1 - e^{-D/D_0})^n$$

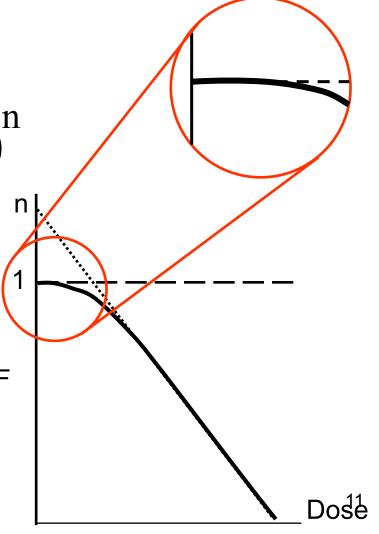
- Assumes random damage
- Probability of target remaining undamaged is e^{-D/D_0}
- 1 hit/cell at dose D₀
- When D is large, $S \rightarrow ne^{-D/D_0}$
- Extrapolation number n = the number of targets per cell
- Quasi threshold dose: $D_q = D_0 \cdot \ln(n)$

Single Hit, Multi-Target Model

$$S = 1 - (1 - e^{-D/D_0})^n$$

PROBLEM

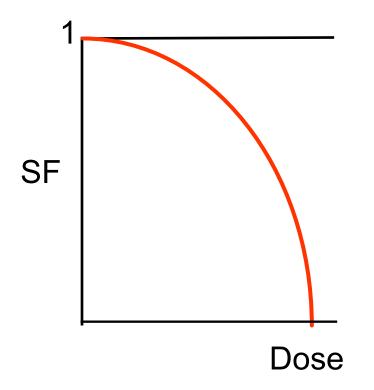
- As D \rightarrow 0, slope \rightarrow 0
- Implies there is no cell SF killing at smallest dose
- Experimental data does not support this

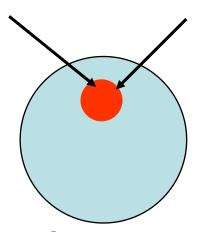


Two Hit, Single Target Model

- A cell contains one target
- A single hit is not sufficient to kill the cell
- $S = e^{-\beta D^2}$

- Cells are killed if the target is hit twice
- Two hits come from two separate particles
- Mean number of lethal events per cell is proportional to D²





β is the probability of a sublethal event

fails at lowest doses:

as D \rightarrow 0, slope \rightarrow 0

Two Component Model

- Assumes cells can be killed in two ways:
 - a single lethal event
 - accumulation of sub-lethal events
- Assumes the two methods are independent ⇒ S = S₁·S_n
- This model is introduced to get agreement with experimental data for $D \rightarrow 0$

$$S_1 = e^{-D/_1D_0}$$
 (where $_1D_0$ relates to single hit lethality)

and

$$\left(S_n = 1 - \left(1 - e^{-D/_n D_0} \right)^n \right)$$
 (where $_n D_0$ relates to sub-lethality)

assuming the single hit, multi-target model,

$$S_{n} = e^{-\beta D^{2}}$$
 assuming the two hit, single target model.

Two Component Model

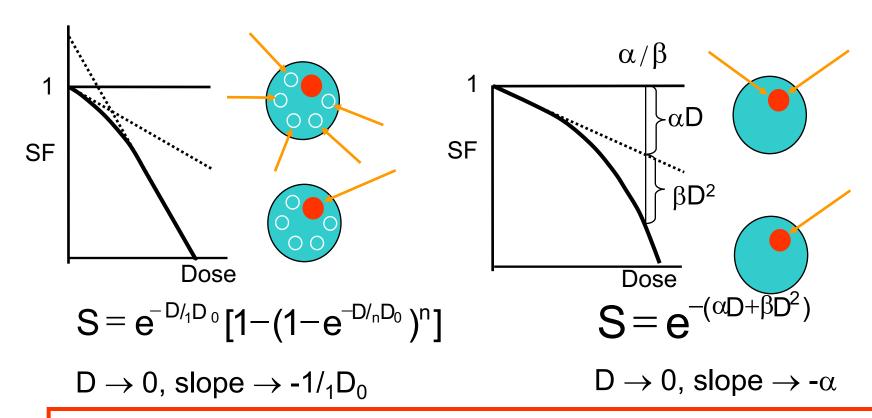
So the survival curve is represented by

$$S = e^{-D/_1D_0} \left[1 - \left(1 - e^{-D/_nD_0} \right)^n \right]$$

or

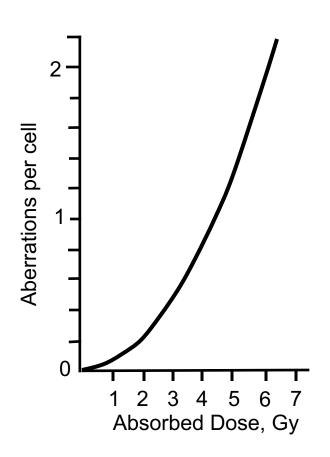
$$S = e^{-(\alpha D + \beta D^2)}$$
 where $\alpha = 1/_1D_0$

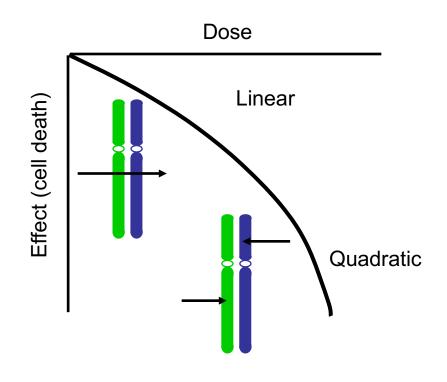
Two Component Model



Statistical uncertainty of experimental data does not allow to distinguish between these two variations of two-component model⁵

Chromosome Aberrations: Dicentrics & Rings



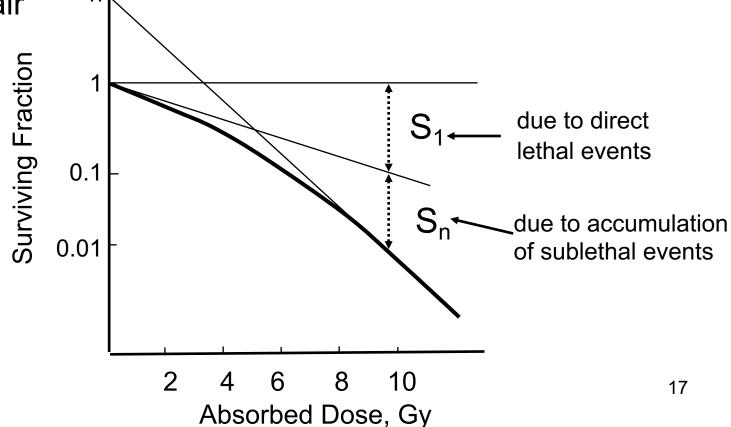


Data for human lymphocytes irradiated by γ-rays

Survival Curve

- For very small doses Surviving Fraction is approximately S₁
- For larger doses contribution of sublethal effects become increasingly important
- S₁ depends only on the total dose D

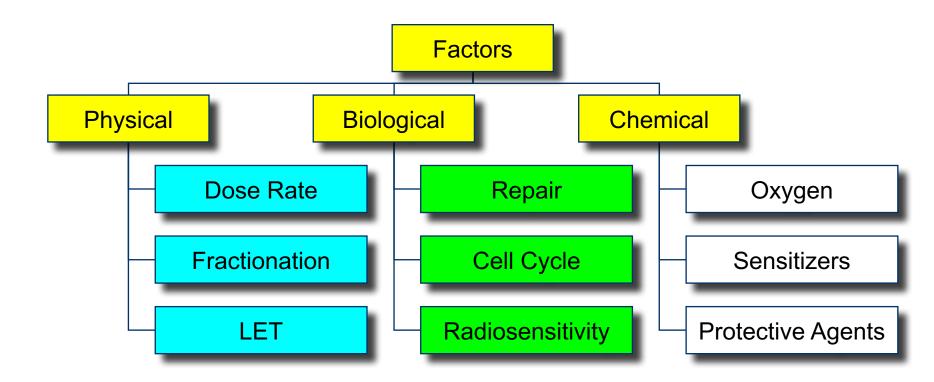
S_n depends on fractionation of radiation and dose rate owing to cellular repair



Models Based on Intracellular Repair

- Two types of lesions: directly lethal and potentially lethal but susceptible to repair
- Repair requires action of enzymatic system and suitable time
- The shoulder on survival curve arises when the repair system is fully operative, only at low doses
- Repair enzyme might become saturated as the dose is increased
- When the repair system is completely saturated, the survival curve becomes exponential

Factors Affecting Radiation Effects

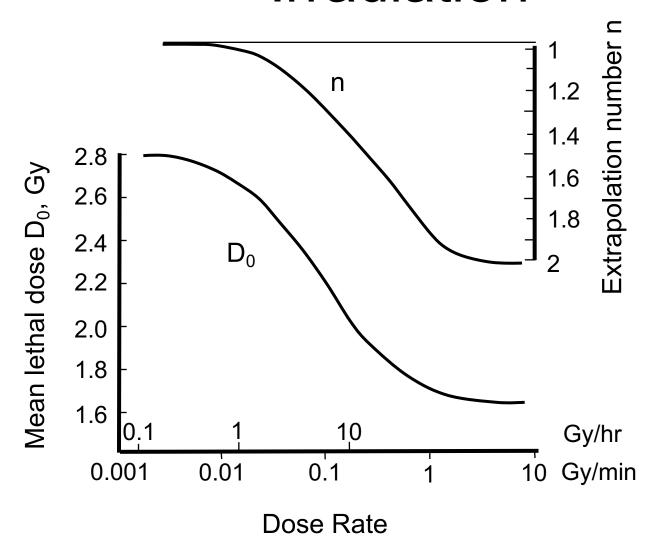


Dose Rate for Continuous Irradiation

- Survival fraction increases as dose rate is reduced over a range of 1.0 - 0.01Gy/min
- This is due to repair of sub-lethal lesions during irradiation
- For high dose rate (>1Gy/min) irradiation is too short to allow for repair
- For very low dose rate (<1Gy/hr) all sub-lesions are repaired. Killing is due to lethal lesions only and Surviving Fraction curve has no shoulder

Dose Rate for Continuous Irradiation 1 for γ -rays 0.1Gy/hr 0.1 0.2Gy/hr 0.3Gy/hr SF 0.02Gy/min .2Gy/min 0.01 0.4Gy/min Results in-vivo 0.001 1Gy/min 7Gy/min 2 4 6 10 12 14 16 Absorbed Dose, Gy

Dose Rate for Continuous Irradiation



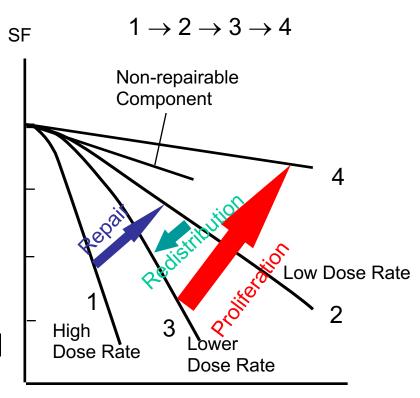
Dose Rate for Continuous Irradiation

- Dose rate is important for radiation effects when the fraction of cells killed is great so that sub-lethal damage contributes significantly to cell killing
- In brachytherapy continuous irradiation during hours/days/weeks is used. Dose rate is very important here
- For external beam radiotherapy with doses about 2Gy per fraction delivered within a minute the dose rate has <u>little</u> importance

Inverse Dose-Rate Effect G2

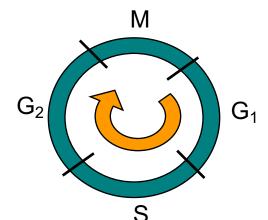
 G_2 G_1 G_1

- As the dose rate is reduced, more sub-lethal damage is repaired, but cells are "frozen" in their positions in the cell cycle and do not progress
- As the dose rate is further reduced, SF curve steepens again because cells can progress through the cycle to pile up at a block in <u>radiosensitive</u> phase G₂ and cannot divide (<u>pre-mitotic</u> <u>block</u>)
- The function of the G₂ pause in cell cycle is to allow a check of chromosome integrity before mitosis is attempted



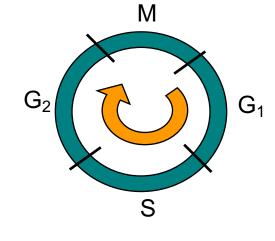
Dose

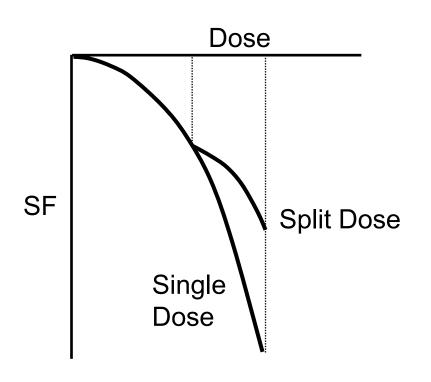
Inverse Dose-Rate Effect G2

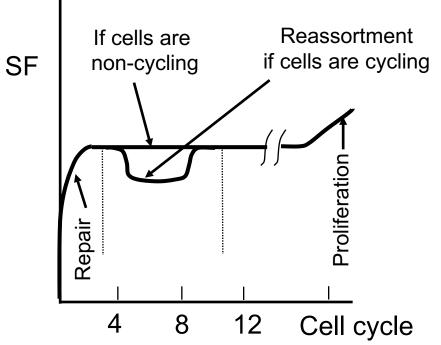


- Molecular checkpoint genes may block the cells in G₂ phase after cells are exposed to any DNA damaging agent
- This is <u>inverse dose-rate effect</u>: decreasing the dose rate results in increased cell killing (valid for dose rates around 0.3-0.4 Gy/h for <u>some</u> cell lines)
- A further lowering of dose rate allows cells to escape radiosensitive G₂ block and divide. Cell proliferation may occur and SF becomes shallower as cell birth from mitosis offsets cell killing from radiation
- Continuous irradiation is more damaging to cells with longer cycles, because a larger dose is absorbed per cell cycle

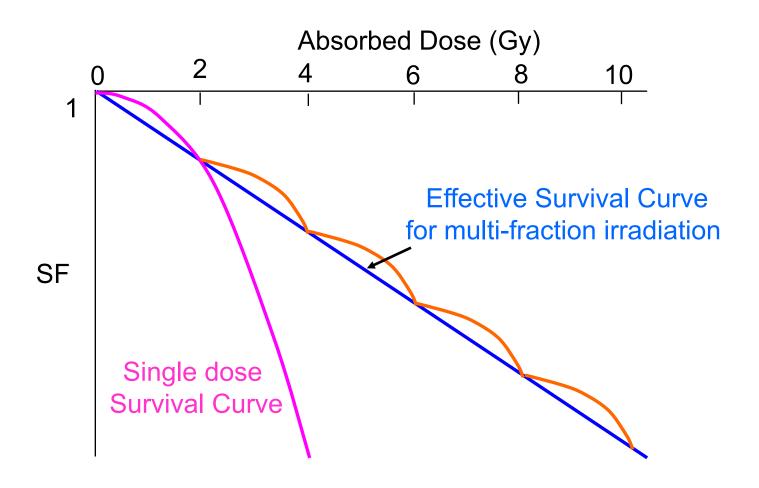
- Dose in fractions has a reduced effect
- SF curve for a fraction is superimposed on preceding fraction and has the same initial slope and the same shoulder ⇒ shallow curve
- Sub-lethal damage is repaired between fractions
- Repair of sub-lethal damage takes place with a half-life of 0.5 - 1.5 hours, depending on cell type
- At least 6 hours separation between fractions should be used for allowing the repair of normal tissues surrounding the tumour (in practice 5 daily fractions of 2Gy are given during external beam therapy per week)







Time between two fractions of radiation (hours)



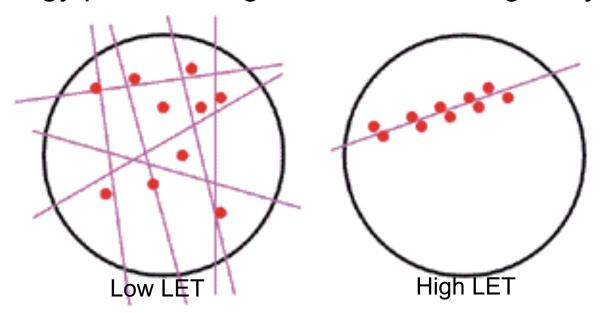
- If survival s is the same for each fraction, the total SF after N fractions is s^N
- For small dose per fraction, only get lethal lesions and sub-lethal damage is repaired between fractions
- The shoulder of the SF curve is repeated many times, so that the effective SF curve in semilogarithmic scale is a straight line from the origin through a point on a single-dose SF curve corresponding to a daily dose fraction (e.g. 2 Gy)
- Resulting curve is exponential $S_{eff} = e^{-\alpha D}$
- The slope reduces as fractions become smaller

Linear Energy Transfer (LET)

LET is the <u>average</u> energy **dE** locally imparted to the medium by a particle of specified energy per unit distance **dI** (keV/ μ m):

LET = dE/dI

LET can be only an average quantity, because at microscopic level, the energy per unit length of track varies greatly



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Linear Energy Transfer

| Radiation | LEI (KeV/μm) |
|---------------|--------------|
| 1 MeV γ– rays | 0.2 |
| 250 kV X-rays | 2.0 |

| 10 MeV protons | 4.7 |
|----------------|-----|
|----------------|-----|

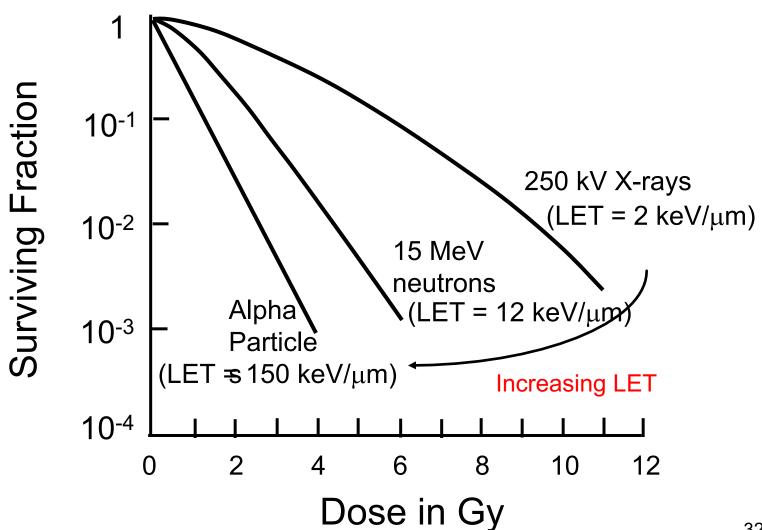
| 15 MeV neutrons 12 | 12 |
|--------------------|----|
|--------------------|----|

2.5 MeV
$$\alpha$$
-particles 166

For a given type of particle, the higher the energy, the lower the LET

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LET

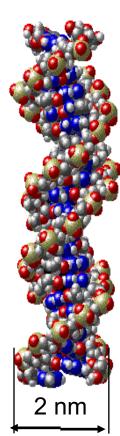


$$\begin{array}{ccc}
\text{LET} & S = e^{-(\alpha D + \beta D^2)}
\end{array}$$

- Survival curve becomes steeper with higher LET
- Shoulder at low LET disappears at high LET
- Implies high LET radiation inactivates cells by single hit whereas low LET radiation requires interaction of sub-lethal hits
- No reduced cell killing with fractionation at high LET
- In terms of linear-quadratic model, increase of LET represents a progressive increase in the linear component (αD) relative to quadratic component

Optimal LET

- Radiations with LET = 100 keV/μm are optimal for producing biological damage in mammalian cells
- At this optimal LET, the average separation between ionising events coincides with the diameter of mammalian DNA double helix (2nm) ⇒ the highest probability of causing double-strand break by passing a single particle
- Radiations having optimal LET = 100 keV/μm include
 - neutrons of few hundred keV
 - low-energy protons
 - high-energy α -particles
- For higher LET (e.g. 200 keV/ μ m) double-strand breaks are readily produced, but the energy is "wasted" because the ionising events are too close together



Relative Biological Effectiveness (RBE)

Biological effect of some radiation **r** is compared with biological effect of 250 kV x-rays that are used as a standard:

$$RBE = D_{250}/D_{r}$$

where RBE is Relative Biological Effectiveness,

D₂₅₀ and D_r are dose of 250 kV x-rays and dose of radiation **r** required for equal biological effect

Relative Biological Effectiveness versus LET

For LET = 100 keV/μm RBE for mammalian cells reaches maximum

